





#### Modeling Brain Diseases with Nonlinear Dynamical Systems to Optimize Medical Treatments

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## Happy 70<sup>th</sup> anniversary Marko







## **Outline** *"Modeling Brain Diseases with Nonlinear Dynamical Systems to Optimize Medical Treatments"*

- Mathematical modeling is a crucial tool for understanding the fundamental mechanisms of the human & animal brain.
- Models based on ordinary differential equations can capture and describe the dynamic interactions between neurons within specific brain regions or across different brain areas.
- We present recent studies demonstrating the usefulness of these models in computationally understanding and mitigating symptoms of two brain diseases:
  - > Parkinson's disease (Part I) and
  - > Epilepsy (Part II)

#### Part I - Parkinson's disease

#### **Clinical motivation**

**Parkinson's disease** (loss of neurons  $\rightarrow$  dopamine): Neurodegenerative disease of the **substantia nigra** that results in a characteristic tremor at rest and a general paucity of movement.

#### pathological neuronal synchrony

#### PD patient, 48ys tremor right hand



post-operative, directly before CR stimulation

#### **Treatment with Neuromodulation**

Coordinated Reset (CR) neuromodulation means to: consecutively deliver brief pulses to different locations of the brain to sequentially reset the phases of the different stimulated subpopulations.



- CR neuromodulation intends to induce a desynchronization which starts a process of unlearning of both pathological neuronal synchrony and pathological synaptic connectivity.
- CR neuromodulation can be applied via electrical stimulation (invasive; e.g. DBS) or via sensory stimulation (non-invasive; e.g. acoustic, vibro-tactile,



Tass PA, Biol. Cybern. 89:81 (2003) / Tass PA, Prog. Theor. Phys. Suppl. 150:281 (2003)

#### Vibrotactile Coordinated Reset Stimulation Induces <u>Sustained Cumulative</u> Benefits in Parkinson's Disease



**Hypothesis**: Taking into account **structural plasticity** reveals **memory-type effects** of the network's treatment susceptibility.

#### Brain scales



#### Which neuron model to choose?

## A brief comparison of the neuro-computational properties of spiking and bursting models



**FL**oating-point **O**perations **P**er **S**econd: a measure of computer performance

#### Phase space

Dynamical system:  $\dot{x} = f(x)$ 

Attractors capture all the characteristics of the activity of the system: steady state, periodic, quasiperiodic and chaotic.



#### A model for Deep Brain Stimulation



#### 11

1000

STN neurons GPe neurons

25

4 1999

15

-5

0

2 cycles off

time (ms)

600

800

400

#### STN/GPe network - Terman-Rubin model



#### Spike timing-dependent plasticity (STDP)

Synaptic plasticity: the ability of synapses to strengthen or weaken over time, in response to increases ( $\uparrow$ ) or decreases ( $\downarrow$ ) in their activity.

The **synaptic weights** *w*<sub>*ij*</sub> are **dynamical variables** that depend on the time

difference  $\left(\Delta t_{ij} = t_j^f - t_i^f\right)$  between the firing (onset) of the **post- and pre-**

synaptic spikes  $(t_i^f \& t_i^f)$ . "Cells that fire together  $\rightarrow$  wire together"



- We restrict the synaptic weights (within the STN neurons) on the interval, avoiding in this way a non-physiological unbounded increase or decrease.
- The (de)synchronized dynamics are **stable** with the above rule and parameter values resulting in **multistability** ( $\rightarrow$  multiple stable equilibrium points).

#### **Structural plasticity**

**Physical creation/deletion** of synapses (during **brain development**, **learning** and **recovery after lesions**).

Synaptic elements (axonal boutons and dendritic spines) grow and recede following homeostatic rules based on the mean electrical activity/firing rate (FR) of the neuron:  $\int \frac{FR(t)}{dEP} = \frac{FR(t)}{r} + \beta$ , if the neuron fires

dFR

dt

synaptic elements/ms

0.0

Gaussian growth rate:

$$\frac{dz}{dt} = v_{\rm SP} \left[ 2e^{-\left(\frac{{\rm FR}(t)-\xi}{\zeta}\right)^2} - 1 \right]$$

*z*: number of synaptic elements  $v_{\text{SP}}$ : max. amplitude of the growth rate  $\zeta = \frac{\varepsilon - \eta}{2\sqrt{\ln 2}}, \quad \xi = (\varepsilon + \eta)/2$ 

The global connectivity is updated on a <u>much slower timescale</u> than changes in electrical activity.

Butz M, van Ooyen A, *PLoS Comput. Biol.* 9:e1003259 (2013) Diaz-Pier S et al., *Frontiers in Neuroanatomy*, 10(57):1662 (2016)

$$\begin{cases} \tau_{SP} \\ -\frac{FR(t)}{\tau_{SP}}, & \text{otherwise} \\ \beta: \text{ calcium intake const.} \\ \tau_{SP}: [Ca] \text{ decay time const.} \\ \tau_{SP}: [Ca] \text{ decay time const.} \\ 1.0 \\ 0.5 \\ 0.0 \\ -0.5 \\ -0.5 \\ -0.5 \\ -1.0 \\ -0.5 \\ -1.0 \\ -0.5 \\ -0.5 \\ -1.0 \\ -0.5$$

2.0

firing rate (Hz)

4.0

#### The Kuramoto order parameter

- One measure of synchrony is the Kuramoto order parameter (R) that indicates the level of synchrony of a collection of phase oscillators.
- We define the order parameters simply by averaging the complex numbers that represent the phase of the oscillators on the unit circle.
- Solution  $\beta$  Given a collection of *N* phase oscillators with phases  $\theta_j$  for j = 1, 2, ..., N, the positions of the oscillators on the unit circle are represented by the complex numbers  $e^{i\theta_j}$ , we define the **Kuramoto order parameter** as:

$$R(t) = \frac{1}{N} \left| \sum_{j=1}^{N} e^{i\theta_j} \right|$$



#### **CR sequences with only STDP versus STDP+SP**



By combining **STDP+SP**, we increased the plasticity potential of the system to explore <u>different connectivity</u> <u>configurations</u>, allowing **long-term structural changes** and **short-term learning** in the **same simulation**.

(A) only STDP only STDP GPE 0.75 CR ON R(t) 0.5 PS ON 0.25 0.0 0 2 4.5 7 0 2 4.5 7 time (min) 0 2 4.5 7 (B) time in minutes ~ 3 months time in minutes ~ 3 months STN 1 GPE mean 1 0.75CR ON 2 R(t) 2 SP ON 2 PS ON 0.25time in minutes time in time in 3 3 3 arb. units arb. units 0.0 024.57time **(C)** ~ 3 months ~ 3 months STN GPE mean 0.75CR ON R(t) 0.5SP ON PS ON 0.256 min 10 min 0.0 024.57024.57time

MT, Diaz-Pier S, Tass PA, Front. Physiol. 12:716556 (2021)

STN neurons
 GPe neurons

### Part II - Epilepsy

#### **Epilepsy**

- Common neurological disorder.
  Epileptic seizures:
  - $\rightarrow$  Excessive electrical discharges.
- Epileptic seizures arise from an imbalance in the regulation of excitation and inhibition.
- Symptoms: language troubles, motor troubles, loss of consciousness etc.



CA: Cornu Ammonis (an earlier name of the hippocampus) DG: Dentate Gyrus

- □ 30-40% of the patients are drug resistant: resective surgery. Resection of the entire **Epileptogenic Zone** (EZ).
- $\Box \ Challenge \rightarrow optimization of the resection.$
- □ Anti-seizure drugs → suppress epileptiform spikes and improve synaptic and cognitive function.
- $\Box$  Neuromodulation  $\rightarrow$  manages seizure propagation.

#### In this work:

■ We computationally study <u>how</u> the **location of an EZ area** and its **connectivity** relevance in the network <u>are</u> <u>related</u> to **widespread seizure propagation** in a mice brain.

- □We search for <u>strategies</u> that can **confine widespread seizures** by either:
  - removing the minimum amount of brain tissue (by blocking certain connections in the network) or
  - suppress the hyperexcitation (loosely mimicking an anti-seizure drug or neuromodulation effect).

#### Large brain simulations



- Computational platform: The Virtual Brain
- Rodent species are often regarded as suitable analogues for humans due to the significant similarities in brain structure and connectivity between the two.
- Mice brain Structural Connectivity from the Allen Institute.



#### **The Epileptor model**

$$\dot{x}_{1,i} = y_{1,i} - f_1(x_{1,i}, x_{2,i}) - z_i + I_1,$$
  
 $\dot{y}_{1,i} = 1 - 5x_{1,i}^2 - y_{1,i},$ 

$$\dot{z}_i = \begin{cases} r(4(x_{1,i} - x_{0,i}) - z_i - 0.1z_i^7) + K \sum_j c_{ji}(x_{1,i} - x_{1,j}) & \text{if } z_i < 0, \\ r(4(x_{1,i} - x_{0,i}) - z_i) + K \sum_j c_{ji}(x_{1,i} - x_{1,j}) & \text{if } z_i \ge 0, \end{cases}$$

$$\dot{x}_{2,i} = -y_{2,i} + x_{2,i} - x_{2,i}^3 + I_2 + 0.002g(x_{1,i}) - 0.3(z_i - 3.5), \quad (4)$$
$$\dot{y}_{2,i} = \frac{1}{\tau}(-y_{2,i} + f_2(x_{2,i})), \quad (5)$$

 $\dot{g}(x_{1,i}) = -0.01(g(x_{1,j}) - 0.1x_{1,i}),$ where

$$f_1(x_{1,i}, x_{2,i}) = \begin{cases} 3x_{1,i}^3 - x_{1,i}^2 & \text{if } x_{1,i} < 0, \\ (x_{2,i} - 0.6(z_i - 4)^2)x_{1,i} & \text{if } x_{1,i} \ge 0, \end{cases}$$

and

 $f_{2}(x_{2,i}) = \begin{cases} 0 & \text{if } x_{2,i} < -0.25, \\ 6(x_{2} + 0.25) & \text{if } x_{2} \geq -0.25. \end{cases}$ (8) **Phenomenological model:**  $(x_{1,i}, y_{1,i}, z_{i}) \text{ bursting neuron (fast)} \\ (x_{2,i}, y_{2,i}) & \text{ spiking neuron (slow)} \\ x_{2}-x_{1}: & \text{mimics the membrane potential} \\ z: \text{ slow permittivity (dictates how close the system is to the seizure threshold)} \end{cases}$ 



#### The Epileptor model: bifurcation diagram



#### The Epileptor model: Epileptogenic Zone (EZ)

- **Epileptogenicity** *x*<sub>0</sub> defines the distance to SN bifurcation.
- **Propagation Zone (PZ)**  $(x_0 < -2.06)$ : healthy brain areas.



Seizures are generated by either a **localized** production of excessive discharges occurring in **one area or hemisphere** (*focal*), or simultaneously in both **hemispheres** (*generalized*), that can **either remain localized or propagate** in the brain network (widespread seizure).

#### **Seizure propagation:** <u>widespread</u> seizure

- Network of coupled Epileptors
- Epileptogenic Zone: left field CA1 rem

focal seizures: seizures that start in one brain area and may or may not remain localized



#### **Seizure propagation:** <u>localized</u> seizure

- Network of coupled Epileptors
- Epileptogenic Zone: left field CA3



#### **Connectivity properties of the EZs**

• Testing all possible EZ of the Allen SC + 20 varied connectomes



#### Widespread seizure prevention

Z: I CA1

6000

5000

4000.5

3000 Ĕ

dista

1000 <sup>Ĕ</sup>

#### **Standard resection strategy:**

Removal of a small portion of the brain.



- •Memory and language
- •Visual impairment
- •Depression/mood changes
- •Headache
- •Stroke

#### **Our strategies:**

Minimal modification of the brain structure:

- **Selective** edge resection (milder surgical approach)
- **EZ outgoing weight** reduction
  - (neuromodulation approach)

#### Widespread seizure prevention



#### Widespread seizure prevention with edge removal Resection strategies:

• Blocking pathways in both hemispheres

**Case II** 

Removing the strongest connection





Case III



Courson, Quoy, Timofeeva, MT Front. Comput. Neurosci. 18:1360009, 2024

7000

6000

5000

4000

3000

2000

1000

# EZ connectivity after edge resection and outgoing weight reduction – CA1



# EZ connectivity after edge resection and outgoing weight reduction - DG



Courson, Quoy, Timofeeva, MT Front. Comput. Neurosci. 18:1360009, 2024

#### **Take home messages**

#### Nonlinear Dynamical Systems can model brain healthy and diseased brain activity and be used to optimize medical treatments

#### Part I (Parkinson's Disease)

- Therapy and rehabilitation can employ structural plasticity to counteract maladaptive plastic changes and ultimately restore brain function.
- Structural plasticity reveals memory-type effects of the network's treatment susceptibility and predict dosage-dependent phenomena relevant for clinical studies.

#### Part II (Epilepsy)

- ➤ Seizures can be kept constrained around the EZ region → selectively removing (blocking) specific connections informed by the structural connectome and graph network measurements or by locally reducing outgoing connection weights of EZ areas.
- Such approaches may help in minimizing surgical or medical intervention while simultaneously preserving the original structural connectivity and maximizing brain functionality.

# <section-header>CollaboratorsParkinson's studyPer Ar BrasPer Ar Ar BrasPre Ar Bras<td

#### Articles

- Manos T., Diaz-Pier S., Tass P.A. Front. Physiol. 12:716556, 2021
- Courson J, Quoy M., Timofeeva Y., Manos T. Front. Comput. Neurosci. 18:1360009, 2024

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#### Thank you for your attention!